



End-to-end tests using alanine pellets read by EPR in a heterogeneous phantom for radiotherapy treatments

DE LA RECHERCHE À L'INDUSTRIE



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The aim of Radiotherapy treatments is to deliver the dose to the tumor with an accuracy of absorbed dose < 5% and to spare healthy tissues.



Context



Tissue density variations



Laboratoire National

Dose calculation in low density medium and using small size photon beam is challenging for Treatment Planning System (TPS) algorithms

Present work consists in :

Evaluation of AAA and Accuros algorithm performances / E2E test using Alanine-EPR technique



Dosimetry principle using alanine pellets read using an Electronic Paramagnetic Resonance (EPR) Spectrometer



central pic amplitude is

proportional to the unpaired electron then to the dose

Alanine is an amino acid (protein peptide chain)

Radiolysis of alanine



Radical concentration proportional to the dose







X band Elesxys EPR spectrometer

Alanine radicals are very stable the sample can be reread several times, it is tissue equivalent.

- Alanine pellets have a small size (Ø = 5 mm, h = 3 mm)
- The irradiated alanine EPR signal is linear with dose
- It is dose rate independent
- It has a negligible energy dependence for photon beams (1 MeV 18 MeV)
- •It has a wide dose range (1 \rightarrow 100 000 Gy)

Drawbacks:

- It has to be stored in a dark and dry room
- The readout is delayed

Champ magnétique (G)

Alanine dosimeters are used as secondary dosimeters

Calibration curve establishment



Alanine irradiation in in IAEA TRS 398 reference conditions using a medical accelerator













Typical uncertainty of a 40 Gy irradiated alanine pellet is equal to 1.2 % (k = 1)



Medical accelerator calibration control at cancer centre ICO in Angers (France)



The first step of the end to end process is to check the beam calibration



Alanine Irradiation at ICO Hospital



Alanine Irradiation at LNHB

A calibration curve has been done in both sites at LNHB and at ICO Hospital in reference conditions (IAEA 398TRS) Calibration curves

Medical accelerators Varian Truebeam 6 MV

Alanine pellets are read at LNHB

The two calibration curves are very linear and in excellent agreement

The deviation between the slope of the two calibration curves is below 1 %. There is a very good agreement with a coverage factor k = 1

The ICO hospital beam calibration is validated



| | Calibration Relative | |
|--------------|----------------------|-------------|
| | curve slope | uncertainty |
| LNHB | 0,308 | 0,54% |
| ICO Hospital | 0,306 | 1,09% |

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End-to-end tests consist in the process validation of the patient whole treatment



The aim of these tests in the present work are to

Check that the delivered dose corresponds to the prescribed dose within 5%

Compare 2 TPS algorithm performances where a lack of electronic equilibrium is encountered for a small field size and an heterogeneous phantom





The IMRT Thorax Phantom CIRS 002LFC is recommended by IAEA for the clinical commissioning tests (TECDOC 1583)



Special inserts for tissue, lung and spine adapted to our alanine pellet container were developed



Each insert is inserted in its dedicated region

5 irradiations conditions were studied



Tissu : T

Lung : L and tissue insert in lung (RL)

Bone/Spine : S and tissue insert in spine (TS)

Additionally we made irradiations by using the tissue insert in the lung region (TL) and also in the bone region (TS) in order to check the algorithms calculation performances





Tissu insert in tissu region (T)Lung insert in lung region (L)Tissu insert in lung region (TL)Bone insert in spine region (S)Tissu insert in bone region (TS)

All irradiation configurations were irradiated using a 6 MV beam energy, 10 x 10 cm²

| | | beam size | - |
|---|---------------------|--|---|
| Tissue and Bone Treatment plans Lung treatment plans DCAI treatment plan | | VMAT treatment using a Planning Target Volume (PTV) was the 4 alanine pellets | |
| | | 8 beam angles static irradiation PTV was the Phantom insert Leafs conformed close to the phantom insert | |
| - | DCAT treatment plan | 8 beam angles static irradiation PTV was the 4 alanine Leafs conformed close to the alanine container Small field (2.5 cm x 1 cm) | |



VMAT in Tissu



VMAT in Spine





8

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Eclipse 15.8. Version TPS algorithms

(AAA), Analytical Anisotropic Algorithm

(Acuros XB), Advanced Dose Calculation algorithm

Deterministic solution of the linear Boltzmann transport equation (LTBE)

Absorbed dose to water

Dose calculation grid size : 1 mm³

For both algorithms, the alanine electronic density was entered in the TPS (HU determined using the electronic density and the scanner correspondence curve (HU = f(Ed))

Alanine-EPR absorbed dose to water determination (EGS4 cavity)

Alanine dose measurement using EPR is the dose in the alanine medium

A transfer factor has been calculated (using EGS4 MC code) for the dose to water determination

$$D_{w,Q_{clin}} = \frac{(D_{w,Q_{clin}})_{MC}}{(D_{al,Q_{clin}})_{MC}} D_{al,Q_{clin}}$$





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TPS **AAA**/EPR dose to water discrepancies

BoneTissueLungAll discrepancies between AAA calculation and the alanine EPRmeasurement do not exceed 5 % except for lung DCAT clinical TPS

DCAT irradiation was also done in lung but using the tissue insert in lung and it does agree with alanine measurements

This result reveals a difficulty for the AAA algorithm to manage a calculation in a light material as the lung in a small static field



TPS **AXB**/EPR dose to water discrepancies

All discrepancies between AXB calculation and the alanine EPR measurement do not exceed 5 %

AXB TPS dose to water calculations agree with alanine-EPR measurements within their uncertainties (k = 2).

Uncertainties are calculated with a coverage factor k = 2



Measurements were done at the hospital in the same phantom irradiation configurations using a IBA ionisation chamber

Ionization chamber: CC04 (IBA)

- Cavity volume: 0.4cc
- Cavity length: 3.6 mm
- Cavity diameter: 4 mm

Inserted in specifically designed inserts (lung, tissue, bone)





$$D_{w,Q_{clin}} = M_{Q_{clin},corr}^{f_{clin}} N_{D,w,Q_0}^{f_{ref}} k_{DO}$$

 $M_{Q_{clin},corr}^{f_{clin}}$ reading of the ionization chamber corrected from background, temperature, pressure, polarity effect and ion recombination

 N_{D,w,Q_0}^{fref} cross-calibration coefficient from a reference chamber directly calibrated at LNE-LNHB (no k_{Q,Q_0} because the reference chamber is directly calibrated for the TPR_{20,10} of the linac)

 k_{DO} daily output of the linac

But clinical measurements are far from reference measurements (Field size and heterogeneous phantom)







Discrepancies between EPR and IC measurements in spine region equal to around 7 %

Discrepancy in lung region with the lung insert for small field equal to 20 % for DCAT treatment plan

measurement

On the contrary to alanine, IC calibration coefficient changes when the beam size changes (mainly due to the dosimeter density which not water equivalent and to the fact that the phantom density which is very different to the reference conditions).

Monte Carlo simulations are needed in order to investigate these discrepancies

End to end tests were undertaken at an hospital using EPR alanine dosimeters in an heterogeneous phantom

Beam calibration in reference conditions verification

The calibration of the hospital facility has been validated by establishing a calibration curve, that was in full agreement with the LNHB reference calibration curve.

« End-to-end » tests were carried out using a Thorax phantom

- Difficulties of the AAA algorithm to deal with the calculation of the dose in the presence of a light material like lung and a small field has been identified.
- The E2E test was validated for all configurations using the Acuros AXB algorithm of the Eclipse TPS

Next step

Implement end-to-end quality assurance for stereotactic radiotherapy using alanine dosimeters









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Thank you for your attention

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