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# Determination of consensus $k_Q$ values for megavoltage photon beams for the update of IAEA TRS-398

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# Abstract

The IAEA is currently coordinating a multi-year project to update the TRS-398 Code of Practice for the dosimetry of external beam radiotherapy based on standards of absorbed dose to water. One major aspect of the project is the determination of new beam quality correction factors,  $k_Q$ , for megavoltage photon beams consistent with developments in radiotherapy dosimetry and technology since the publication of TRS-398 in 2000. Specifically, all values must be based on, or consistent with, the key data of ICRU Report 90.

Data sets obtained from Monte Carlo (MC) calculations by advanced users and measurements at primary standards laboratories have been compiled for 23 cylindrical ionization chamber types, consisting of 725 MC-calculated and 179 experimental data points. These have been used to derive consensus  $k_Q$  values as a function of the beam quality index TPR<sub>20,10</sub> with a combined standard uncertainty of 0.6%. Mean values of MC-derived chamber-specific  $f_{ch}$  factors for cylindrical and plane-parallel chamber types in <sup>60</sup>Co beams have also been obtained with an estimated uncertainty of 0.4%.

# **1. Introduction**

The writing of the first edition of the IAEA TRS-398 Code of Practice (Andreo et al 2000) for the dosimetry of external beam radiotherapy based on standards of absorbed dose to water was completed in the mid-1990s. A number of developments in radiotherapy techniques and dosimetry have taken place since that date, or will be implemented in the near future, which justify the need for updating the Code of Practice. Some of the more relevant aspects that require consideration in an update of TRS-398 are:

- (a) New ionization chamber types have become commercially available that require beam quality correction factors,  $k_Q$ , for their use according to the recommendations of TRS-398. This requires an update of the list of ionization chamber types, some of them being already relatively old or even no longer available. Additionally, an extensive experimental study by McEwen (2010) revealed that not all chamber types originally listed in TRS-398 can be considered "reference class ionization chambers".
- (b) The implementation of new radiotherapy technologies, mostly related to megavoltage (MV) photon beams, protons and heavier ions, whose reference dosimetry requires guidance and data for end users. There have been significant developments in linear accelerator technology and flattening-filter free (FFF) photon beams have become widely used. Their reference dosimetry (for 10 cm× 10 cm fields), described in the IAEA TRS-483 Code of Practice for small static fields, (Palmans et al 2017, Palmans et al 2018), needs to be taken into account while maintaining consistency with the recommendations of TRS-483.
- (c) The publication of ICRU Report 90 on Key Data for Ionizing–Radiation Dosimetry (Seltzer et al 2016), recommending new values for the most relevant fundamental quantities and corrections. The impact of the new data on ionization chamber calibrations by standards laboratories and on beam quality correction factors for the different radiation modalities needs to be taken into account. Recent publications by Czarnecki et al (2018), Mainegra-Hing and Muir (2018) and Pimpinella et al (2019) on  $k_Q$  factors for MV photon beams have shown small differences between the use of ICRU Report 37 (Berger et al 1984) and ICRU Report 90 data, but consistency throughout the dosimetry chain requires the use of the latter.
- (d) The Monte Carlo (MC) simulation of radiation transport has become a widely used technique for the accurate calculation of dosimetric quantities for all beam types, superseding many of the approximations used to determine the data in TRS-398.
- (e) In the dosimetry of kilovoltage (kV) x rays, not only the previsions of TRS-398 for the ready availability of  $N_{D,w}$  calibrations for these beams have not become a reality, but also there were no specific data recommended to users. New data for the dosimetry of low- and medium-energy kV x rays using ICRU-90 data have been published (Andreo 2019).

An IAEA project was initiated to update TRS-398. A core working group was formed in 2016 with the task of re-writing relevant sections of text in TRS-398, coordinating the MC calculations and measurements at standards laboratories of beam quality correction factors made by different international research groups, and analysing their results to produce a consensus set of data for the different radiation modalities. For MV photon beams, one of the major objectives was to determine  $k_Q$  values averaged over data obtained by the research groups using different Monte Carlo codes and experimental data measured in laboratories having independent absorbed dose to water standards.

The purpose of this work is to summarize the methodology followed to derive consensus values of photon beam quality correction factors and their estimated uncertainty, to provide the parameters for a functional fit to the  $k_Q$  data available for a large number of ionization chamber types as a function of the photon beam quality index TPR<sub>20,10</sub>, and to make available tabulated values of  $k_Q$ . Mean values of Monte Carlo-derived  $f_{ch}$  (<sup>60</sup>Co) chamber-specific factors for cylindrical and plane-parallel ionization chambers are also included. All the reported values are consistent with the key data given in ICRU Report 90 for graphite, water and air, whereas data from previous ICRU reports have been used for other materials.

#### 2. Background

#### **2.1.** The $k_{Q,Q_0}$ formalism

The beam quality correction factor,  $k_{Q,Qo}$ , is defined in the formalism of IAEA TRS-398 as the ratio of the calibration coefficients of an ionization chamber in terms of absorbed dose to water at the beam qualities Q and  $Q_0$ :

$$k_{Q,Q_0} = \frac{N_{D,W,Q}}{N_{D,W,Q_0}}$$
(1)

where  $Q_0$  is the reference beam quality used by the standards laboratory. Values specifically measured for a particular user chamber should be used when available. In most cases, however, such data is not available and calculated  $k_{Q,Q_0}$  values must be used. In the current edition of TRS-398, for conditions where the Bragg–Gray cavity theory is applicable, values of  $k_{Q,Q_0}$  were calculated using the general expression (Andreo 1992):

$$k_{Q,Q_0} = \frac{(s_{w,air})Q}{(s_{w,air})Q_0} \frac{(p_{ch})Q}{(p_{ch})Q_0} \frac{(W_{air})Q}{(W_{air})Q_0}$$
(2)

where  $s_{w,air}$  is the Spencer-Attix water-to-air stopping-power ratio,  $p_{ch}$  is the overall chamber perturbation correction factor, and  $W_{air}$  is the average energy to create an ion pair in dry air, all for the beam qualities Q and  $Q_0$ .

For MV photon beams, values of were calculated using data from ICRU Report 37 (Berger et al 1984) and the value of was 33.97 eV for photons and electrons. Due to the lack of consistent data for the different components entering into the chamber perturbation correction factor (i.e. cavity perturbation, , displacement effect, , wall effect, , and central electrode correction, , see TRS-398), some values were derived from experiment, others by old MC or analytical calculations, and in some cases taken to be unity.

Since the publication of TRS-398, advanced MC techniques have been developed that enable the detailed simulation of ionization chambers and radiation sources (<sup>60</sup>Co  $\gamma$ -ray units and clinical accelerators) with great efficiency. Rather than calculating independently  $s_{w,air}$  and chamber perturbation factor components for a given beam quality and ionization chamber, Sempau et al (2004) proposed computing directly within the MC simulation the factor

$$f_{\rm ch}(Q) = \left[\frac{D_w(P)}{D_{ch-air}}\right]_Q \quad (3)$$

where  $D_w(P)$  is the dose to a point in water (in practice, calculated for a very small volume), and  $D_{ch-air}$  is the mean absorbed dose in the chamber cavity. Note that no specific components of chamber perturbation correction factors are explicitly included in this factor and the constraint of small and independent components of  $p_{ch}$  required by cavity theory is no longer needed. The procedure in equation (3), which can be referred to as a global  $f_{ch}(Q)$  that includes  $s_{w,air}$  and all possible chamber perturbation components, irrespective of their size or interrelation (i.e. not being small and independent), has become the currently accepted MC calculation approach. It differs from the approach used by other authors, see, e.g. Paskalev et al (2002) and Capote et al (2004), where instead of the dose to a point,  $D_w(P)$ , the dose to water is calculated in a volume identical to that of the chamber cavity,  $D_w$ (vol). This alternative in fact leads to the calculation of the correction for the chamber volume averaging effect,  $k_{vol}$ , and has been used in some of the MC data contributed to this work.

From equations (2) and (3), the beam quality correction factor becomes defined as:

$$k_{Q,Q_0} = \frac{(f_{\rm ch})Q}{(f_{\rm ch})Q_0} \frac{(W_{air})Q}{(W_{air})Q_0}$$

which using the reference quality  $Q_0$  of <sup>60</sup>Co  $\gamma$  rays and noting the constancy of  $W_{air}$  for high-energy photons and electrons, yields

$$k_Q = \frac{f_{\rm ch}(Q)}{f_{\rm ch}(^{60}{\rm Co})}$$

As opposed to the method for obtaining separately  $s_{w,air}$  and  $p_{ch}$  values, the approach to compute  $f_{ch}(Q)$ , of which the product  $(s_{w,air} p_{ch})Q$  is an approximation, as a single quantity in a MC simulation has important advantages. In addition to both  $f_{ch}$  for  $k_Q$  in equation (5) being independent of the intrinsic approximations involved in cavity theory, the main advantage of an MC calculation of  $f_{ch}$  is that its uncertainty is considerably smaller than that resulting from combining the uncertainties of  $s_{w,air}$  and of  $p_{ch}$ , where the values and their uncertainties are derived indirectly and independently.

There has been controversy on the constancy of  $W_{air}$  for high-energy radiotherapy beams since the mid 1980s. Should this quantity vary with energy, its influence would be intrinsically accounted for in  $k_Q$  measurements and, for consistency, MC calculations would need to be corrected for the variation. However, it should be emphasized that the ICRU Report 90 includes an in-depth review of the historical measurements and recent analysis made, concluding that  $W_{air}$  does not show a significant dependence with electron energy above a low-energy threshold (see figure 5.4 in ICRU-90), the spread of the data being consistent with the stated uncertainty of 0.12 eV (0.35%).

#### 2.2. ICRU-90 key data

The ICRU Report 90 (Seltzer et al 2016) on key data for measurement standards in radiation dosimetry has reviewed the quantities and correction factors that play a fundamental role in dosimetry, estimated the uncertainties of key data and analysed the implications of the new recommended data on measurements and calculations. The new key data has been endorsed by the CCRI (McEwen et al 2017) and at its meeting in 2019 the National Metrology Institutes (NMIs) have committed to adopt ICRU-90 by the end of 2019 or by early 2020. Hence, the adoption of ICRU-90 data will be relatively rapid and comprehensive, and will in turn be implemented in standards laboratories for the calibration of ionization chambers.

ICRU-90 includes values of fundamental quantities entering into the determination of stopping powers for light- and heavy-charged particles. It provides recommendations for the mean excitation energy, the *I*-value, of air (85.7 eV), graphite (81 eV) and water (78 eV), and for the grain mass density of graphite to be used when evaluating the density effect (2.265 g cm<sup>-3</sup>) in the mass electronic stopping power. These quantities yield new stopping power values for electrons and positrons, protons and light ions (alpha particles and carbon ions) and, indirectly, also change the average energy required to produce an ion pair for protons and carbon ions. The recommended values for  $W_{air}$  are 33.97 eV for electrons (which is constant above about 10 keV) and 34.44 eV for protons; for carbon ions the value is subject to the same increase as for protons (0.6 %, assuming negligible perturbation correction factors for the chambers used in its determination), i.e. the resulting  $W_{air}$  is estimated to be 34.71 eV.

The state of the art and current trends regarding photon cross sections and mass energy-absorption coefficient values and ratios are analysed in detail, but no specific data were recommended in ICRU-90 due to issues related to the photoelectric and Compton effects, where various options are available. Other key data, such as the heat defect of liquid water and the radiation chemical yield for the Fricke dosimeter, and the correction to account for the charge of the initial electrons set in motion by low-energy photons, have also been reviewed.

The impact of the new data on measurement standards, and therefore on ionization chamber calibrations by standards laboratories, varies depending on the radiation modality and type of standard used. The changes are up to about 0.8 % for air-kerma standards for kV x-ray and <sup>60</sup>Co beams (also for some brachytherapy sources, e.g. <sup>192</sup>Ir). A similar change could have been expected for the ionometric absorbed dose to water standard for <sup>60</sup>Co at the BIPM (reference for the IAEA Dosimetry Laboratory), but the implementation of the new data is assessed in the context of known changes to other correction factors resulting in a change of only 0.1 %. For graphite-calorimetry standards there are only small

changes, mostly associated with the transfer methods used for converting dose in graphite to dose in water, which depends on the particular standard at each laboratory. No changes occur for water calorimetry.

### **3. Materials and methods**

#### **3.1. Determination of** *k*<sub>Q</sub> **values**

As already mentioned,  $k_Q$  values for MV photon beams were determined by different research groups worldwide, these being advanced MC users and standards laboratories, yielding comprehensive sets of new data for a large number of ionization chamber types. Details on the derivation of  $k_Q$  values by some of the research groups can be found in the Extended Synopses of the IAEA Symposium on 'Standards, Applications and Quality Assurance in Medical Radiation Dosimetry (IDOS 2019)<sup>1</sup> and in recent and submitted publications by Czarnecki et al (2018), Mainegra-Hing and Muir (2018), Pimpinella et al (2019), Tikkanen et al (2020), Giménez-Alventosa (2020), etc.

Beam quality correction factors were determined by MC calculations according to equation (5), and by measurements at standards laboratories following equation (1). The beam qualities used were  $TPR_{20,10}$  values between 0.6 and 0.8 approximately, 25 MeV being the highest energy; this range is considered to be representative of that widely used in the clinic.

For the experimental values, primary standards of absorbed dose to water based on water and graphite calorimetry were used; information on the standard used at each laboratory can be found in the on-line BIPM key comparison database (http://kcdb.bipm.org/) and the references therein. Waterproof sleeves generally of PMMA were used for chambers that are not waterproof, although the sleeve thickness varied for the different laboratories (typically not more than 1 mm). The stated standard uncertainties for the measured  $k_Q$  values were in the range from 0.3% to 0.5%.

The MC systems used were EGSnrc (Kawrakow et al 2019a) and Penelope (Salvat 2014), usually in conjunction with the user codes *cavity* (Kawrakow et al 2019b), *egs\_chamber* (Wulff et al 2008) and *penEasy* (Sempau et al 2011). The MV radiation sources were phase–space files for different conventional (with flattening filter, WFF) and FFF linacs, and in some cases published spectra for several linacs (Mohan *et* al 1985, Sheikh-Bagheri and Rogers 2002, Capote et al 2006, Brualla et al 2019). For <sup>60</sup>Co  $\gamma$  rays the most common source were spectra of therapy or laboratory units (Mora et al 1999, Burns 2003), although in some cases specific phase–space files for particular units were used. Details on the geometries of the individual ionization chamber types were in most cases provided by the respective manufacturers. In all cases the MC groups obtained  $k_Q$  values with Type A standard uncertainties of the order of 0.15%.

To verify the homogeneity of the MC calculations, all the groups were requested to calculate  $k_Q$  values for a NE-2571 Farmer-type ionization chamber in photon beams of different qualities. For this purpose, a detailed NE report was distributed to the groups (Nuclear Enterprises 1984) to minimize the influence of using different geometry descriptions. The goal was to establish the degree of variation of the kQ values when implementing a common chamber geometry as a result of the different MC transport parameters and codes used by each group.

For the reference dosimetry of FFF beams the update of TRS-398 will introduce an additional chamberreading correction  $k_{vol}$  to account for the volume averaging effect whenever the beam profile across the detector is not homogeneous, a correction discussed in detail in TRS-483. This choice has been preferred over the alternative of providing different  $k_Q$  values for FFF and WFF photon beams, as is done in TRS-483. Special linacs such as CyberKnife, MR-linacs etc, have not been included in the

<sup>&</sup>lt;sup>1</sup> www.iaea.org/sites/default/files/19/06/cn-273-book-extended-synopses.pdf

compilation of data because either their use is rather limited or those delivering small fields are already considered in TRS-483. Note also that the current edition of TRS-398 includes recommendations for the dosimetry of radiotherapy beams in non-standard conditions, i.e. for beam dimensions different from the  $10 \text{ cm} \times 10 \text{ cm}$  reference field size. The update will maintain the recommendations and include new developments, particularly for the dosimetry of small MV fields in TRS-483, providing a consistent framework for these conditions.

Equation (5) shows that all calculations require  $f(Q_0)$  data for the reference quality of <sup>60</sup>Co  $\gamma$  rays, which were provided separately by some of the groups; the goal was to produce a harmonized common data set to be used with other radiation modalities also based on <sup>60</sup>Co as the reference quality (electrons, protons and heavier ions).

#### **3.2.** Analysis of the data

A total of 725 MC-calculated and 179 measured data points were compiled for the 23 cylindrical chamber types analysed, see table 1. The two sets of beam quality factors for each chamber type were combined to obtain statistically-based consensus  $k_Q$  values and their uncertainty estimates, the latter referring to the relative standard uncertainty (k = 1) expressed as a percentage.

	Number of da	ata points	Chamber-type specific parameters				
Ionization chamber type	Monte Carlo	experimental	a	b			
Capintec PR-06C Farmer	10	3	1.06 833	-0.08 262			
Exradin A1SL Miniature	14	6	1.21 633	-0.13 351			
Exradin A12 Farmer	35	6	1.09 783	-0.09 544			
Exradin A12S Short Farmer	16	3	1.11 499	-0.10 057			
Exradin A18	10	3	1.10 487	-0.09 670			
Exradin A19 Classic Farmer	29	6	1.12 024	-0.10 493			
Exradin A26	10	3	1.09 587	-0.09 383			
Exradin A28	19	3	1.12 453	-0.10 278			
IBA CC13	42	6	1.11 441	-0.10 260			
IBA CC25	10	3	1.08 981	-0.09 254			
IBA FC23-C Short Farmer	19	3	1.09 189	-0.09 346			
IBA FC65-G Farmer	64	20	1.09 752	-0.09 642			
IBA FC65-P Farmer	42	3	1.12 374	-0.10 784			
NE 2561/2611A Secondary Standard	20	19	1.07 699	-0.08 732			
NE 2571 Farmer	126	28	1.08 918	-0.09 222			

	Number of da	ata points	Chamber-type specific parameters					
Ionization chamber type	Monte Carlo	experimental	a	b				
PTW 30 010 Farmer	25	3	1.12 594	-0.10 740				
PTW 30 011 Farmer	15	0	1.10 850	-0.10 107				
PTW 30 012 Farmer	25	13	1.12 442	-0.10 415				
PTW 30 013 Farmer	65	23	1.18 273	-0.13 256				
PTW 31 010 Semiflex	29	6	1.23 755	-0.15 295				
PTW 31 013 Semiflex	48	6	1.19 297	-0.13 366				
PTW 31 016 PinPoint 3D	15	0	1.11 650	-0.10 841				
PTW 31 021 Semiflex 3D	37	13	1.29 612	-0.16 514				
Total number of determinations	725	179						

**Table 1.** Chamber types and number of Monte Carlo-derived and experimental  $k_Q$  determinations for high-energy photon beams of different qualities. The two rightmost columns correspond to the values of the chamber-type specific parameters *a* and *b* obtained from the different fits using equation (6).

For each chamber type, the combined data set of MC and experimental values was fitted using a module developed with version 10 of *Mathematica* (Wolfram Research Inc. 2016), having the empirical functional form

$$k_Q \left( TPR_{20,10} \right) = \frac{1 + \exp\left(\frac{a - 0.57}{b}\right)}{1 + \exp\left(\frac{a - TPR_{20,10}}{b}\right)} \tag{6}$$

where *a* and *b* are specific parameters for each chamber type, and the nominal value 0.57 is taken to represent the TPR<sub>20,10</sub> value typically measured for a <sup>60</sup>Co  $\gamma$ -ray unit (forcing  $k_Q = 1$  for this reference quality). This value is included in the figures below, but it should be noted that considering the TPR<sub>20,10</sub> of <sup>60</sup>Co  $\gamma$ -ray beams in parallel with values for MV photon beams is a convenient but not rigorous approach, as the photon spectra from a radionuclide and from bremsstrahlung are substantially different.

The sensitivity of the  $k_Q$  fits to the TPR<sub>20,10</sub>(<sup>60</sup>Co) value used was tested for the five chambers having the largest number of data points (see figures 1 and 2) using the lowest (0.568) and highest (0.578) values found in the literature for TPR<sub>20,10</sub>(<sup>60</sup>Co). As the lowest value is very close to the nominal value 0.57 used for the fits, the analysis was focused on the upper limit, obtained from the BJR-25 data (Aird et al 1996). For MV beams having TPR<sub>20,10</sub> = 0.6, which is approximately the lowest beam quality used in the MC and experimental  $k_Q$  determinations, the maximum difference in the fitted  $k_Q$  value using the nominal and the highest TPR<sub>20,10</sub>(<sup>60</sup>Co) was 0.05%, being below this difference for TPR<sub>20,10</sub> > 0.6. The influence of the TPR<sub>20,10</sub>(<sup>60</sup>Co) value used in the  $k_Q$  fits was therefore considered to be negligible.



**Figure 1.** Values of  $k_Q$  for megavoltage photon beams obtained from Monte Carlo calculations by different research groups (open circles) and measured at standards laboratories (filled circles) for a NE-2571 Farmer-type ionization chamber. The solid line is a fit to the total of 154 data points using equation (6) and the dashed lines are the 95% prediction limits of the fit. The short-dashed line corresponds to the fit of the 28 experimental data points.



**Figure 2.** Values of  $k_Q$  for megavoltage photon beams obtained from Monte Carlo calculations by different research groups (open circles) and measured at primary laboratories (filled circles) for the Farmer-type chambers IBA FC65-G, PTW 30013 and Exradin A12, and the PTW 31013 Semiflex chamber type. The solid lines are fits to the combined data set using equation (6) and the dashed lines are the 95% prediction limits of the fit.

The parameters *a* and *b* of the best  $k_Q$  fit to the combined MC and measured data sets were determined for each chamber type. The standard deviation of the experimental data with respect to the combined fit was corrected statistically (see section 5) and taken as the standard uncertainty of the fit for each chamber type. The mean value for all the chamber types contributed to the overall standard uncertainty estimation. Prediction limits of the fits at the 95% level were also determined and plotted in the figures (note that these do not represent the prediction limits for the consensus  $k_Q$  values given in this report; the  $k_Q$  uncertainties are discussed in section 5).

#### 4. Results and discussion

#### 4.1. High-energy photon beams

The  $k_Q$  results obtained for the NE-2571 Farmer-type chamber are shown in figure 1, which includes a fit to the combined 126 MC-calculated and 28 measured data points, yielding a root mean square (rms) difference of the data about the fit of 0.2%. It can be seen that most results agree within about  $\pm 0.5\%$ , showing consistency in the different determinations for this common chamber type. The differences in the MC-calculated  $k_Q$  factors for this chamber type were not significant, indicating no systematic dependence on the particular MC system (EGSnrc versus PENELOPE) or specific user code parameters. The figure includes a fit to the measured data alone, which practically coincides with the combined fit. Also shown are the 95% prediction limits for the combined fit, which for this chamber type with a relatively large data set are significantly narrower than those arising from the uncertainties for the consensus  $k_Q$  values discussed in section 5, which are based on the deviations of the experimental data from the combined fit. Observe also that some experimental data points at TPR<sub>20,10</sub> values greater than about 0.73 appear slightly below the -95% prediction limits, a trend that appears also in the fits for other chamber types and remains to be explained.

As mentioned above,  $k_Q$  data were supplied by different contributors and standards laboratories. Many of the  $k_Q$  measurements and MC simulations were carried out within the EURAMET 16NRM03 RTNORM project (Pinto 2019); other significant data sets were the comprehensive experimental set of McEwen (2010) and MC data by the NRCC group (Muir and Rogers 2010, Muir et al 2011, Mainegra-Hing and Muir 2018). On the other hand, the extensive set of  $k_Q$  measurements by Seuntjens et al (2000) have not been included in the compilation because the NRC beams used at that time, generated with aluminium targets and filters combined with magnetic sweeping for flattening, had substantially different spectral characteristics compared with those of current clinical linac beams.

For the MC-calculated and experimental  $k_Q$  data sets, consensus values were determined for 23 ionization chamber types and different beam qualities. It should be noted that some of these chamber types (Exradin A28, PTW 31 021) have not yet been shown to be reference-class according to the criteria by McEwen (2010) and one chamber type (PTW 31 016) has been shown to not exhibit reference-class behaviour. Table 1 shows the chamber types and number of MC-derived and experimental  $k_Q$  determinations. Values of the chamber-type specific parameters *a* and *b* obtained from the combined fit using equation (6) for the different chamber types are included in the table. The rms difference of the data about the fits varied between 0.05% and 0.4%, yielding an average of 0.23%.

Regarding FFF beams and the effect of volume averaging on chamber response, it should be noted that all experimental determinations entering into  $k_Q$  are corrected for volume averaging (either explicitly or implicitly). Hence, ignoring possible spectral differences, an FFF beam and a WFF beam of the same

 $\text{TPR}_{20,10}$  should have approximately the same experimental value for kQ. This assertion has been verified experimentally by e.g. DePrez et al (2018), finding differences of less than 0.23% (uncertainty smaller than 0.35%) for eight Farmer-type ion chambers of three different models in 6 MV and 10 MV paired WFF and FFF beams having the same TPR<sub>20,10</sub> in each case. In contrast, the MC calculations for FFF beams have taken different approaches such that volume averaging is not always treated in the same way. Furthermore, different input spectra have been used, some derived from full phase-space calculations and others using a simplified source that might not contain realistic beam profile information. Despite these differences, the scatter of the combined MC results for FFF and WFF beams does not show any significant effect arising from this heterogeneous treatment of volume averaging, being consistent with the estimated uncertainties of this work. This agrees with the findings of recent publications (Lye et al 2016, Czarnecki et al 2018). It can therefore be concluded that the consensus  $k_0$  values provided in this work, obtained by combining experimental and MC results, can be used equally for WFF and FFF beams having the same TPR<sub>20,10</sub> without significant additional uncertainty. Users of FFF beams should, on the other hand, correct their dosimeter readings by a volume averaging correction,  $k_{\rm vol}$ , which parallels the procedure used for chamber calibration at standards laboratories.

Examples of  $k_Q$  data and their fits for some of the ionization chamber types commonly used, namely the Farmer-types IBA FC65-G, PTW 30 013 and Exradin A12, and the PTW 31 013 Semiflex, are shown in figure 2. As for the NE-2571 chamber type, some experimental data fall slightly below the -95% prediction limits of the overall fit.

Beam quality correction factors are given in table 2 for different TPR<sub>20,10</sub> values. They have been calculated with equation (6) using the chamber-type specific parameters *a* and *b* given in table 1. It is emphasized that the  $k_Q$  values provided here do not distinguish possible chamber-to-chamber variations of a given chamber type (see, e.g. Andreo et al (2013)) and their use does not preclude the possibility that an individual chamber deviates from the expected behaviour, leading to a source of error that is circumvented when the values are measured at a standards laboratory for a specific user chamber. For waterproof chambers, the  $k_Q$  values provided assume that no waterproof sleeve is used. The use of a PMMA sleeve 1 mm in thickness increases the  $k_Q$  value by up to 0.3% at the highest energies. For non-waterproof chambers, the  $k_Q$  values provided are appropriate for a 1 mm PMMA sleeve.

Chamber type	0.50	0.53	0.56	0.59	0.62	0.65	0.68	0.70	0.72	0.74	0.76	0.78	0.80	0.82
Capintec PR-06C Farmer	1.001 4	1.000 9	1.000 3	0.9993	0.998 0	0.996 1	0.993 4	0.990 9	0.9878	0.983 9	0.9790	0.9727	0.964 9	0.9551
Exradin A1SL Miniature	1.003 2	1.002 0	1.000 6	0.998 7	0.996 5	0.993 6	0.990 1	0.9873	0.984 0	0.980 2	0.9759	0.9709	0.965 2	0.9586
Exradin A12 Farmer	1.002 1	1.001 4	1.000 4	0.9991	0.9973	0.9948	0.991 5	0.988 7	0.985 2	0.9809	0.9756	0.9693	0.961 5	0.952 1
Exradin A12S Short Farmer	1.002 2	1.001 4	1.000 4	0.999 0	0.997 2	0.994 7	0.991 3	0.988 5	0.985 0	0.980 9	0.975 8	0.969 8	0.9624	0.953 7
Exradin A18	1.002 0	1.001 3	1.000 4	0.999 1	0.9973	0.9949	0.9917	0.988 9	0.985 5	0.981 4	0.9764	0.9702	0.962 8	0.953 8
Exradin A19 Classic Farmer	1.002 6	1.001 7	1.000 5	0.998 9	0.996 8	0.994 0	0.9904	0.987 3	0.983 6	0.979 2	0.973 8	0.967 5	0.9599	0.9509
Exradin A26	1.001 9	1.001 3	1.000 4	0.999 1	0.9974	0.995 1	0.991 9	0.989 1	0.985 7	0.981 6	0.976 5	0.9702	0.962 6	0.953 3
Exradin A28	1.002 2	1.001 5	1.000 4	0.9990	0.9972	0.9947	0.9914	0.988 6	0.985 3	0.981 3	0.9764	0.9706	0.963 6	0.9552
IBA CC13	1.002 4	1.001 6	1.000 5	0.998 9	0.9969	0.9942	0.9906	0.9876	0.983 9	0.979 5	0.9742	0.9678	0.960 1	0.9510
IBA CC25	1.001 9	1.001 3	1.000 4	0.9991	0.9974	0.9950	0.991 8	0.9890	0.985 5	0.981 2	0.9760	0.969 5	0.9617	0.952 1
IBA FC23-C Short Farmer	1.002 0	1.001 3	1.000 4	0.999 1	0.9974	0.995 0	0.991 7	0.988 8	0.985 3	0.981 0	0.975 8	0.969 3	0.9614	0.9519
IBA FC65-G Farmer	1.002 2	1.001 4	1.000 4	0.9990	0.9972	0.9946	0.991 2	0.988 2	0.9846	0.980 2	0.9748	0.968 3	0.9603	0.9507
IBA FC65-P Farmer	1.002 8	1.001 8	1.000 5	0.998 8	0.9966	0.9936	0.9897	0.986 5	0.982 6	0.978 0	0.972 5	0.966 0	0.9583	0.949 1
NE 2561/2611A Secondary Standard	1.001 7	1.001 1	1.000 3	0.999 2	0.997 7	0.995 5	0.992 5	0.989 8	0.986 5	0.982 3	0.977 1	0.9706	0.962 7	0.952 8

Chamber type	0.50	0.53	0.56	0.59	0.62	0.65	0.68	0.70	0.72	0.74	0.76	0.78	0.80	0.82
NE 2571 Farmer	1.001 9	1.001 3	1.000 4	0.999 1	0.9974	0.995 1	0.991 9	0.989 1	0.9856	0.981 3	0.976 1	0.9697	0.961 8	0.9522
PTW 30 010 Farmer	1.002 7	1.001 7	1.000 5	0.998 9	0.9967	0.993 8	0.990 1	0.986 9	0.983 2	0.978 7	0.973 4	0.967 1	0.9595	0.9506
PTW 30 011 Farmer	1.002 4	1.001 6	1.000 5	0.998 9	0.9969	0.9942	0.9906	0.987 5	0.983 8	0.9793	0.973 9	0.9674	0.9595	0.950 1
PTW 30 012 Farmer	1.002 4	1.001 6	1.000 4	0.999 0	0.9970	0.9944	0.991 0	0.988 1	0.9846	0.9804	0.9754	0.9694	0.9622	0.9536
PTW 30 013 Farmer	1.004 0	1.002 5	1.000 7	0.9984	0.9956	0.992 0	0.9876	0.984 0	0.9800	0.975 3	0.9699	0.963 6	0.9565	0.9484
PTW 31 010 Semiflex	1.004 6	1.002 9	1.000 8	0.998 2	0.995 2	0.991 4	0.9869	0.983 5	0.979 5	0.975 0	0.9700	0.9643	0.9579	0.9507
PTW 31 013 Semiflex	1.003 8	1.002 4	1.000 7	0.998 5	0.9958	0.9924	0.9882	0.984 8	0.981 0	0.976 5	0.9714	0.965 5	0.9588	0.9511
PTW 31 016 PinPoint 3D	1.003 1	1.002 0	1.000 6	0.998 7	0.9962	0.993 0	0.9888	0.985 3	0.981 2	0.9762	0.9703	0.963 2	0.9549	0.945 1
PTW 31 021 Semiflex 3D	1.004 2	1.002 6	1.0007	0.9984	0.9957	0.9925	0.9886	0.9856	0.9823	0.9786	0.9744	0.9697	0.9645	0.9587

**Table 2.** Calculated values of beam quality correction factors,  $k_Q$ , as a function of the beam quality index TPR<sub>20,10</sub> of megavoltage photon beams, derived with equation (6) using the chamber-type specific parameters *a* and *b* given in table 1.

#### 4.2. <sup>60</sup>Co gamma radiation

All the  $k_Q$  values in TRS-398 and in the present work are based on the reference quality of <sup>60</sup>Co  $\gamma$  rays. For the MC calculations associated with the present work, the global factor  $f_{ch}({}^{60}Co)$ , see equation (5), was determined for each chamber type.

As emphasized in section 2.1, the approach to compute  $f_{ch}({}^{60}Co)$  as a single quantity in a MC simulation, as opposed to obtaining separately  $s_{w,air}$  and  $p_{ch}$  values, has the advantage of a smaller uncertainty than that resulting from combining the uncertainties of  $s_{w,air}$  and  $p_{ch}$  from different sources. Therefore, whereas the use of specific  $s_{w,air}$  and  $p_{ch}$  values is acceptable for proton and heavier ions due to the lack of comprehensive sets of chamber–specific MC-derived  $f_{ch}(Q)$ , values, for the <sup>60</sup>Co data in the denominator of  $k_Q$  the use of  $f_{ch}({}^{60}Co)$ , is preferred as it provides consistency among the high-energy radiation modalities included in TRS-398.

Mean values of MC-calculated  $f_{ch}({}^{60}Co)$ , factors were obtained from 16 data sets (115 data points for the cylindrical chambers in this work as well as nine plane-parallel chambers) extracted from publications and data supplied by different research groups. They are given in table 3 for the different chamber types, for which an average standard uncertainty estimate of 0.4% was obtained. These  $f_{ch}({}^{60}Co)$ , chamber-type specific values are intended to replace the  $(s_{w,air} p_{ch})_{60Co}$  data given in table 37 of the first edition of TRS-398.

Ionization chamber type	$f_{\rm ch}(^{60}{ m Co})$				
Cylindrical chambers					
Capintec PR-06C Farmer	1.104 5				
Exradin A1SL Miniature	1.103 0				
Exradin A12 Farmer	1.106 4				
Exradin A12S Short Farmer	1.104 6				
Exradin A18	1.102 3				
Exradin A19 Classic Farmer	1.1074				
Exradin A28	1.109 5				
IBA CC13	1.109 8				
IBA CC25	1.103 9				
IBA FC23-C Short Farmer	1.107 7				
IBA FC65-G Farmer	1.108 1				
IBA FC65-P Farmer	1.113 5				
NE 2561/2611A Secondary Standard	1.106 2				

Ionization chamber type	$f_{\rm ch}(^{60}{ m Co})$
NE 2571 Farmer	1.108 4
PTW 30 010 Farmer	1.107 2
PTW 30 011 Farmer	1.1129
PTW 30 012 Farmer	1.100 0
PTW 30 013 Farmer	1.108 6
PTW 31 010 Semiflex	1.107 4
PTW 31 013 Semiflex	1.111 0
PTW 31 016 PinPoint 3D	1.1260
PTW 31 021 Semiflex 3D	1.095 1
Plane-parallel cha	umbers
Exradin A10	1.113 7
Exradin A11	1.111 5
Exradin A11TW	1.099 4
IBA NACP-02	1.153 5
IBA PPC-05	1.140 9
IBA PPC-40	1.142 4
PTW Adv. Markus	1.143 4
PTW Markus	1.142 8
PTW Roos	1.141 7

**Table 3.** Mean values of Monte Carlo-derived  $f_{ch}({}^{60}Co)$  chamber-specific factors, approximately equal to the product for  ${}^{60}Co \gamma$ -ray beams. The values were obtained averaging the contribution by different MC groups, yielding an overall standard uncertainty estimate of 0.4%.

# **5.** Estimation of uncertainties of the $k_0$ data

The statistical analysis of the  $k_Q$  values obtained for different ionization chamber types was similar to the procedure used in IAEA TRS-483; it included all the available data sets determined by the various MC and experimental groups. For each chamber type an initial fit was made to the combined data set using equation (6); data points outside the 99.73% (k=3) prediction limits of the fit were filtered out and the fit repeated. Considering that most determinations stated similar relative uncertainties and that these were of different type (combined uncertainties for measured data, Type A uncertainties only for MC data), the various input data sets were not weighted statistically.

The estimation of uncertainties of the  $k_Q$  values was done as follows:

- 1. The MC calculations do not include estimates of Type B uncertainties, and the calculated  $k_Q$  data provided by the different research groups is expected to have correlated uncertainties that do not appear as scatter in their values, which were obtained with the same or similar MC systems. It should be emphasized that the estimation of Type B uncertainties in MC calculations involves considerable difficulty. Although some authors have estimated Type B uncertainties of 0.2%– 0.4% for MV photon beams (Wulff et al 2010, Muir and Rogers 2010), their analysis did not account for components due to the single and multiple electron scattering theories and their implementation in the MC system used, which for years have been considered a major constraint for the MC simulation of ionization chambers (see, e.g. Berger and Wang (1988), Bielajew and Rogers (1988) and Andreo et al (2017)). This constraint also includes the boundary crossing algorithms and the condensed-history step mechanics, which are linked to the implementation of the scattering theories but usually are controlled separately in a MC simulation.
- 2. In contrast, the experimental data for  $k_Q$  provided by different laboratories are largely uncorrelated and deviations from the combined fit evaluated for these data alone provide a more robust basis for an uncertainty estimate. For each chamber type the relative deviation from the fit increased slightly with TPR<sub>20,10</sub>, but the change was small enough to justify adopting an overall quality–independent uncertainty. Fits made for the different chamber types yielded on average a standard prediction uncertainty of 0.51% (reducing to 0.36% when considering only the five chamber types with the most experimental data). This estimate involves (a) the rms deviation  $s_{\rm rms}$  of the measured data with respect to the combined fit, (b) the standard uncertainty *s* including Student's *t* correction

 $s = s_{rms} t_{1-0.68,n-1}$ , as only five chamber types had a large number *n* of measured data points, and (c) the standard prediction uncertainty using  $s_p = s\sqrt{1 + 1/n}$ .

- 3. A contribution was also included for the experimental uncertainty. The rationale for this estimate was that approximately half of the chamber types have only three measured data points, corresponding to one individual chamber measured at one laboratory (three energies), and consequently these data contain no scatter due to the laboratory uncertainties or chamber-to-chamber variations. For each of these chamber types the additional contribution was derived as the mean value of *s* (as in the previous step) for the five chamber types having most measured data points. This mean value of 0.34% is consistent with the range of standard experimental uncertainties for  $k_Q$  stated by the laboratories. A further seven chamber types have data for only two individual chambers, for which a corresponding contribution of  $0.34\sqrt{1/2} = 0.24\%$  was included. The net effect of these additions on the total uncertainty is 0.28%, as indicated in table 4.
- 4. Finally, the uncertainty of assigning  $k_Q$  values to a given photon beam quality was estimated to be 0.2%. This includes uncertainty components for the use of phase-space data files or photon spectra in MC calculations and for any difference in the measurement of  $\text{TPR}_{20,10}$  between the research groups providing the data and the end user (for both WFF and FFF beams).

-- (0/)

Component	$u_c$ (70)
Prediction uncertainty from fit using equation (6)	0.51
Net experimental uncertainty	0.28
Assignment of $k_{\rm Q}$ to TPR <sub>20,10</sub>	0.20
Combined standard uncertainty in $k_Q$	0.62

Commente

**Table 4.** Estimated relative standard uncertainty of the kQ values for megavoltage photon beams.

The different components are summarized in table 4, yielding a combined standard uncertainty for the  $k_Q$  values of high-energy photons obtained in this work of about 0.6%. This uncertainty can be considered a conservative estimate for any of the chamber types listed in table 1. However, as noted in point 2 above, for the five chamber types with the most data the prediction uncertainty is significantly smaller, leading to an overall uncertainty for  $k_Q$  approaching 0.4% when these chamber types are used. The uncertainty of 0.6% does not preclude a future reduction in uncertainty for any chamber type for which significant data becomes available.

#### 6. Summary and conclusions

Beam quality correction factors,  $k_Q$ , for the dosimetry of megavoltage photon beams, contributed by international research groups for the update of the IAEA TRS-398 Code of Practice, have been compiled. The data have been calculated by advanced Monte Carlo users and measured by standards laboratories for 23 ionization chamber types, yielding a total of 725 MC-calculated and 179 experimental data points. This work describes the methods followed to derive consensus  $k_Q$  values, providing fitting parameters and tabulated data for each chamber type as a function of the TPR<sub>20,10</sub> photon beam quality index. Mean values of MC-derived chamber-specific factors for cylindrical and plane-parallel ionization chambers in <sup>60</sup>Co  $\gamma$ -ray beams are also given. All the values provided are based on, or are consistent with, the key data of ICRU Report 90.

The analysis of the  $k_Q$  data yields, on average, rms differences between the input data and the fitted values of the order of 0.2%. There is good data integrity, as all the input data agree with the fits approximately at the 0.5% level; however, some experimental data points at TPR<sub>20,10</sub> greater than about 0.73 fall slightly below the -95% prediction limit, a trend that appears to be systematic, rather than random, and that requires further investigation. The combined standard uncertainty of the consensus  $k_Q$  values is estimated to be 0.6%. It is concluded that the consensus  $k_Q$  values provided in this work can be used equally for WFF and FFF beams having the same TPR<sub>20,10</sub> without significant additional uncertainty.

The updated data sets are expected to contribute to the harmonization and accuracy of radiotherapy beam calibrations based on a systematic and internationally unified approach.

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# References

Aird E G A et al 1996 Central axis depth dose data for use in radiotherapy Brit. J. Radiol. Suppl. (London: The British Institute of Radiology) **25** 

Andreo P 1992 Absorbed dose beam quality factors for the dosimetry of high-energy photon beams Phys. Med. Biol. **37** 2189–2211

Andreo P 2019 Data for the dosimetry of low- and medium-energy kV x rays Phys. Med. Biol. **64** 205019

Andreo P, Burns D T, Hohlfeld K, Huq M S, Kanai T, Laitano F, Smyth V G and Vynckier S 2000 Absorbed dose determination in external beam radiotherapy: An International Code of Practice for dosimetry based on standards of absorbed dose to water Technical Report Series no. 398 (Vienna: International Atomic Energy Agency)

Andreo P, Burns D T, Nahum A E, Seuntjens J and Attix F H 2017 Fundamentals of Ionizing Radiation Dosimetry (Weinheim, Germany: Wiley-VCH)

Andreo P, Wulff J, Burns D T and Palmans H 2013 Consistency in reference radiotherapy dosimetry: resolution of an apparent conundrum when <sup>60</sup>Co is the reference quality for charged-particle and photon beams Phys. Med. Biol. **58** 6593–6621

Berger M J, Inokuti M, Andersson H H, Bichsel H, Dennis J A, Powers D, Seltzer S M and Turner J E 1984 Stopping powers for electrons and positrons ICRU Report 37 (Bethesda, MD: International Commission on Radiation Units and Measurements)

Berger M J and Wang R 1988 Multiple-scattering angular deflections and energy-loss straggling Monte Carlo Transport of Electrons and Photons ed T M Jenkins, W R Nelson, A Rindi, A E Nahum and D W O Rogers (New York: Plenum Press) 21–56

Bielajew A F and Rogers D W O 1988 Electron step-size artefacts and PRESTA Monte Carlo Transport of Electrons and Photons ed T M Jenkins, W R Nelson, A Rindi, A E Nahum and D W O Rogers (New York: Plenum Press) 115–137

Brualla L, Rodríguez M, Sempau J. and Andreo P 2019 PENELOPE/PRIMO-calculated photon and electron spectra from clinical accelerators Radiat. Oncol. **14** 10

Burns D T 2003 Calculation of for <sup>60</sup>Co air-kerma standards using PENELOPE Report CCRI(I)/03-40 (Sèvres: Bureau International des Poids et Mesures)

Capote R, Jeraj R, Ma C-M, Rogers D W O, Sánchez-Doblado F, Sempau J, Seuntjens J and Siebers J V 2006 Phase-Space Database for External Beam Radiotherapy, IAEA Report INDC(NDS)-0484 (Vienna: International Atomic Energy Agency)

Capote R, Sánchez-Doblado F, Leal A, Lagares J I, Arráns R and Hartmann G H 2004 An EGSnrc Monte Carlo study of the microionization chamber for reference dosimetry of narrow irregular IMRT beamlets Med. Phys. **31** 2416–2422

Czarnecki D, Poppe B and Zink K 2018 Impact of new ICRU Report 90 recommendations on calculated correction factors for reference dosimetry Phys. Med. Biol. **63** 12

De Prez L, DePooter J, Jansen B, Perik T and Wittkämper F 2018 Comparison of kQ factors measured with a water calorimeter in flattening filter free (FFF) and conventional flattening filter (cFF) photon beams Phys. Med. Biol. **63** 11

Giménez-Alventosa V, Giménez V, Ballester F, Vijande J and Andreo P 2020 Monte Carlo calculation of beam quality correction factors for PTW cylindrical ionization chambers in photon beams Phys. Med. Biol. submitted

Kawrakow I, Mainegra-Hing E, Rogers D W O, Tessier F and Walters B R B 2019a The EGSnrc Code System: Monte Carlo Simulation of Electron and Photon Transport, NRCC Report PIRS-701 (Ottawa: National Research Council Canada)

Kawrakow I, Mainegra-Hing E, Tessier F, Townson R and Walters B R B 2019b EGSnrc C++ class library, NRCC Report PIRS-898 (Ottawa: National Research Council Canada)

Lye J E, Butler D J, Oliver C P, Alves A, Lehmann J, Gibbons F P and Williams I M 2016 Comparison between the TRS-398 code of practice and the TG-51 dosimetry protocol for flattening filter free beams Phys. Med. Biol. **61** N362

Mainegra-Hing E and Muir B R 2018 On the impact of ICRU Report 90 recommendations on kQ factors for high-energy photon beams Med. Phys. **45** 3904–3908

McEwen M R 2010 Measurement of ionization chamber absorbed dose kQ factors in megavoltage photon beams Med. Phys. **37** 2179–2193

McEwen M R, Burns D T, D'Arienzo M, DePooter J, Pinto M and Rapp B 2017 Report to CCRI(I) on the recommendations of ICRU Report 90 Report CCRI(I)/17-07 (Sèvres: Bureau International des Poids et Mesures)

Mohan R, Chui C and Lidofsky L 1985 Energy and angular distributions of photons from medical linear accelerators Med. Phys. **12** 592–597

Mora G M, Maio A and Rogers D W O 1999 Monte Carlo simulation of a typical <sup>60</sup>Co therapy source Med. Phys. **26** 2494–2502

Muir B R, McEwen M R and Rogers D W O 2011 Measured and Monte Carlo calculated kQ factors: Accuracy and comparison Med. Phys. **38** 4600–4609

Muir B R and Rogers D W O 2010 Monte Carlo calculations of kQ, the beam quality conversion factor Med. Phys. **37** 5939–5950

Nuclear Enterprises N E 1984 The 0.6cc Farmer thimble chamber series, Radiological Application Report No. 3, issues 2 and 3 (Reading, UK: Nuclear Enterprises Ltd)

Palmans H, Andreo P, Huq M S, Seuntjens J and Christaki K 2017 Dosimetry of Small Static Fields used in External Beam Radiotherapy: An IAEA-AAPM international Code of Practice for reference and relative dose determination, Technical Report Series No. 483 (Vienna: International Atomic Energy Agency)

Palmans H, Andreo P, Huq M S, Seuntjens J, Christaki K E and Meghzifene A 2018 Dosimetry of small static fields used in external photon beam radiotherapy: Summary of TRS-483, the IAEA-AAPM international Code of Practice for reference and relative dose determination Med. Phys. **45** e1123–e1145

Paskalev K, Seuntjens J and Podgorsak E B 2002 Dosimetry of ultra small photon fields Recent Developments in Accurate Radiation Dosimetry ed J Seuntjens and P N Mobit (Madison, WI: Medical Physics Publishing) 298–318

Pimpinella M, Silvi L and Pinto M 2019 Calculation of kQ factors for Farmer-type ionization chambers following the recent recommendations on new key dosimetry data Physica Medica **57** 221–230

Pinto M 2019 kQ factors in modern external beam radiotherapy applications to update IAEA TRS-398 Report 16NRM03 RTNORM, EURAMET <u>http://www.rtnorm.eu</u>

Salvat F 2014 PENELOPE-2014: A Code System for Monte Carlo Simulation of Electron and Photon Transport, Report NEA/NSC/DOC(2014) (Issy-les-Moulineaux: OECD Nuclear Energy Agency)

Seltzer S M, Fernández-Varea J M, Andreo P, Bergstrom P M, Burns D T, Krajcar-Bronic I, Ross C K and Salvat F 2016 Key Data for Ionizing Radiation Dosimetry: Measurement Standards and Applications ICRU Report 90 (Bethesda, MD: International Commission on Radiation Units and Measurements)

Sempau J, Andreo P, Aldana J, Mazurier J and Salvat F 2004 Electron beam quality correction factors for plane-parallel ionization chambers: Monte Carlo calculations using the PENELOPE system Phys. Med. Biol. **49** 4427–4444

Sempau J, Badal A and Brualla L 2011 A PENELOPE-based system for the automated Monte Carlo simulation of clinacs and voxelized geometries Med. Phys. **38** 5887–5895

Seuntjens J P, Ross C K, Shortt K R and Rogers D W O 2000 Absorbed-dose beam quality conversion factors for cylindrical chambers in high energy photon beams Med. Phys. **27** 2763–2779

Sheikh-Bagheri D and Rogers D W O 2002 Monte Carlo calculation of nine megavoltage photon beam spectra using the BEAM code Med. Phys. **29** 391–402

Tikkanen J, Pimpinella M, Zink K, Teles P, Borbinha J, Ojala J, Siiskonen T and Pinto M 2020 Calculated beam quality correction factors for ionization chambers in MV photon beams Phys. Med. Biol. **65** 075003

Wolfram Research Inc. 2016 Mathematica, Version 10 ()

Wulff J, Heverhagen J T, Zink K and Kawrakow I 2010 Investigation of systematic uncertainties in Monte Carlo-calculated beam quality correction factors Phys. Med. Biol. **55** 4481–4493

Wulff J, Zink K and Kawrakow I 2008 Efficiency improvements for ion chamber calculations in high energy photon beams Med. Phys. **35** 1328–1336