International Workshop on radiosensitization

Modeling and experimental validation of radiation - Cell interaction in radiotherapy by photon activation of gold nanoparticles

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Summary

• Context

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- State of the art of gold nanoparticle photoactivation therapy
- Physics and Monte-Carlo simulation
- First results of simulation with Penelope code
- Conclusion and prospect

• Current limitations of radiotherapy:

- The tolerance of healthy tissues
- The inability of irradiation techniques to treat diffused cancers (ex: Glioblastomas).
- Concept of heavy element enhanced radiotherapy :
 - Irradiation with a low energy X-ray beam (50 150 keV) in the presence of high Z elements.
 - Enhancement of the dose effect in the tumor loaded with high Z element and creation of complex damages at the cellular level.

• Goals:

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- Understand physical phenomena connected to these enhancement effects using Monte Carlo simulation and experimental measurements (provided by ESRF).
- Focus here on gold nanoparticles (GNP).
- Use of different physical parameters as emitted electrons spectra and Dose Enhancement Factor (DEF).

State of the art : GNP photoactivation therapy

- Study of Hainfeld et al. (Phys. Med. Biol (2004)) :
 - Very good survival response, up to enhancement of 4, by treating cancerous mice combining injection of GNP of 1.9nm and irradiation with a RX tube at 250kVp.
- Hainfeld (Phys. Med. Biol (2010)):
 - New *in vivo* results using the same technique but with synchrotron beam at 68 and 157 keV.



Radiosensitization experiments with GNP (E. Brun et al. 2009):



State of the art : Monte Carlo simulation with GNP

Cho et al. (Phys. Med. Biol. (2005)):

- Attempt to reproduce Hainfeld's results.
- Model representing a tumor embedded with a gold-water mixture.
- Obtained a DEF of 2.1 into the tumor.
- → Need a model which takes into account the distribution of GNP and microdosimetry.

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State of the art : Monte Carlo simulation with GNP

- Zhang et al. (Biomed Microdevices (2009)):
 - Comparison of calculated macroscopic dose with two different model:
 - Homogeneous gold-water mixture (Cho's 2005 method).
 - Structure with gold nanoparticles.

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 The homogeneous gold-water model overestimates the dose until 16% in the target volume. → Confirm the need of modelling the nanostructures.

State of the art : Monte Carlo - track structure code

• Previous macroscopic studies show the importance of:

- Modelling geometries and calculating doses at a micro and nano level.
- Finding parameters more relevant than physical dose to describe the phenomena.
- Monte Carlo codes called "track structure" can be used to simulate very precisely electron and photon transport. Main codes:
 - Penelope: adapted for clinical radiation dosimetry and transport description of low energy X-Ray and electrons.
 - EGS: adapted for clinical radiation dosimetry.

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- MCNPx: not precise to model relaxation cascades (in development).
- G4: developed for high energy physics, now extended to all radiation physics (project : G4DNA).

Some are used to describe interaction of particles with DNA :

- Ftacnikova et al. (Radiation Protection Dosimetry (2000))
- Terrissol et al. (Int. J. Radiat. Biol. (2008))
- Nikjoo et al. (Radiation Protection Dosimetry (2006))



Physics and Monte Carlo simulation

• Monte Carlo method :

 Allow to follow the particles transport in matter according to random processes determined with interaction probabilities.

• Photon interaction :





Atomic relaxation :



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Physics and Monte Carlo simulation

• Electron range in water, ESTAR (NIST databases):



- Range of 10 keV electron \approx 2.5 µm in water, nucleus scale.
- Range of 50 keV electron \approx 40 μ m in water, cellular scale.
- Range of 100 keV electron \approx 140 μ m in water, few cells.

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Penelope code

- Gold nanoparticle geometry, spectrum study:
 - sphere of 100 nm diameter, full of water or gold.
 - Detectors are virtual tools which quantify the spectrum of outgoing particles.



Outgoing photon spectrum for 85 keV monoenergetic beam



→ Fluorescence relaxation well described in Penelope.

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Electron spectrum for 85 keV monoenergetic beam



→ Relaxation cascade and X-ray interaction with shell and sub-shell well described in Penelope.

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Electron spectrum for 68 keV monoenergetic beam 1.00E-05 Gold 1.00E-06 Coster- $L_1 L_2 L_3$ PE e⁻ M,N of Kronig M_{1-5} Water La. LB 1.00E-07 Frequency (1/eV*particle) Auger L-X 1,00E-08 1,00E-09 1,00E-10 1,00E-11 1,00E-12 Mean energy ≈ 35 keV 1,00E-13 1,00E-14 1,00E-15 1,00E-16 10 20 30 40 50 60 0 Electron energy (keV)

→ Modification of the spectra before and after the K-edge: influence on the mean energy and range of electrons created from the GNP.

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Study of total electrons emitted and the yield of low energy electrons (< 10 keV) produced in GNP as a function of beam energy



 \rightarrow Strong enhancement of the yield of low energy electron (range of few µm) after the K-edge due to the photoelectric absorption.

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Mean energy of electrons emitted from the GNP as a function of incident beam energy



 \rightarrow Mean energy of electrons emitted from the GNP increases with the incident beam energy and falls down after the K-edge.

 \rightarrow Optimization of beam energy as a function of the GNP targeting.

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Study of total electrons emitted and the yield of low energy electrons (<10keV) produced in GNP as a function of GNP radius



 $\rightarrow\,$ Total number of electrons relative to the mass of gold seems to decrease as a 1/x² tendency with the GNP radius.

 $\rightarrow\,$ Yield of electrons lower than 10 keV decreases linearly with the GNP radius.

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Study of microdosimetry around the GNP

• Dose study :

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- Geometry: spherical GNP of 100 nm diameter in a water sphere of 1 μm.
- Study of the deposited dose due to the GNP in the water sphere.



Dose profile on the Z axis for a 85keV monochromatic beam



 $\rightarrow\,$ Deposited dose due to the GNP is dominated by the low energy electrons produced.

 \rightarrow Quasi-isotropic diffusion of dose around the GNP at a µm scale.

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DEF calculated as a function of beam energy with a 100 nm GNP

Dose Enhancement Factor = Mean dose in the water sphere with GNP Mean dose in the water sphere without GNP



Mean dose calculated as a function of GNP radius for a 85 keV monochromatic beam



 $\rightarrow\,$ Deposited dose in the 1 μm water sphere due to the GNP increases with the radius as a exponential tendency.

 \rightarrow The increase of electron production for small GNP does not influence the dose at a µm scale.

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Conclusion and prospect

• Conclusion :

- Photoactivation radiotherapy with GNP induces complex dose effects at a cellular level and requires more precise study of the local effect of GNP.
- This study aims understanding physical phenomena correlated to these local effects.
- The characterization of GNP in terms of particles created and local physical dose deposited are described according to the beam energy and the radius of spherical GNP.
- Prospect :

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- Study these local characteristics in a more realistic geometry.
- Experimental measurements planed to study the dependency with beam energy.
- Study different geometries of GNP.
- The challenge is to find a relevant parameter to see correlation between physical data and biological results.