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Tritium radioactive labeling of detonation nanodiamonds

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For the first time, the radioactive labeling of detonation nanodiamonds was efficiently achieved using a tritium microwave plasma. According to our measurements, the total radioactivity reaches 9120±120 □Ci/mg, with 93% of 3H 10 atoms tightly bonded to the surface and up to 7% embedded into the diamond core. Such 3H doping will ensure highly stable radiolabeled nanodiamonds, on which surface functionalization is still allowed. This breakthrough opens the way to biodistribution and pharmacokinetics studies of 15 nanodiamonds, while this approach can be scalable to easily treat bulk quantities of nanodiamonds at low cost.

Nanodiamonds (NDs) possess several essential assets for biomedical applications: a very weak cytotoxicity and ²⁰ genetoxicity¹⁻⁴, a carbon-related surface chemistry allowing covalent functionalization for targeting or labeling (oligonucleotides, proteins, fluorescent dyes...) ^{5,6} and a tunable surface charge for drug adsorption^{7,8}. Detonation nanodiamonds synthetized by explosion ⁹ combine all this possibilities in a

²⁵ primary size of 5 nm, compatible with kidney filtration for an expected easier elimination ¹⁰.

Nevertheless, the prerequisite to any therapeutic applications of NDs vector is the assessment of its toxicity, tissue distribution and elimination. While NDs are now recognized as well tolerated ³⁰ by organisms ^{11,12}, there are still contradictory results regarding their tissue distribution and clearance ^{13,14}. Nanoparticle radiotracers are currently widely used to assess quantitatively the health hazard related to nanotechnologies or as theranostic agents ¹⁵. In the former studies, NDs biodistribution in small animal was

³⁵ inferred from the signal of radiotracers as ¹⁸F ¹⁶,¹⁸⁸Re ¹⁷ or dyes¹⁸ chemically grafted. However, these labels are likely to be separated from NDs during their transit in the animal body and unable from any further functionalization. As such radioactive labeling of the diamond core itself appears as a promising

⁴⁰ "tritium probe" approach that ensures the NDs tracing for biolabeling or biodistribution investigations. Although tritium labeling was previously mentioned ¹⁹, such a direct radioactive labeling using plasma treatment has not been proposed yet.

We report here the radiolabeling of detonation nanodiamonds ⁴⁵ with tritium. Tritium labeling is routinely used for biodistribution studies, for example of paclitaxel encapsulated nanoparticles ²⁰ or squalenoyl nanomedicine²¹. ³H label was also introduced into a drug component to monitor its release by pharmacokinetics studies ²². Indeed, tritium is a β^- emitter, which decays into ³He,

studies ²². Indeed, tritium is a β^{-} emitter, which decays into ³He, ⁵⁰ with a 12.32 years half-life and an average 5.7 keV kinetic energy of the beta particle. Tritium is easily detectable from standard

liquid scintillation counting and autoradiography. In case of stable insertion onto ND vector, the biodistribution will not be affected by tritium labeling and the potential risk of the *in vivo* ⁵⁵ formation of ${}^{3}\text{H}_{2}\text{O}$ would be avoided²³.

Our original approach is based on a microwave (MW) plasma treatment in order to label nanodiamonds with ³H atoms. This experimental technique was previously applied to efficiently hydrogenate detonation NDs ^{24,25} and rely on the hydrogen ⁶⁰ plasma exposure of NDs contained in a quartz pipe. Hundreds of milligrams of NDs can be treated at the same time, resulting in fully hydrogenated NDs (H-NDs). Using this approach, the formation of C-¹H bonds at the ND surface has already been evidenced via different spectroscopic techniques (XPS, FTIR, ⁶⁵ Raman) as reported elsewhere ^{7,25,24}. We also demonstrated

⁶⁵ Raman) as reported elsewhere ^{7,23,24}. We also demonstrated specific surface properties of ¹H-NDs leading to positive Zeta potential in water suspension related to their high affinity toward water molecules ⁷. Note that hydrogen diffusion in the ND core is also expected, as it occurs in bulk diamond under similar plasma

⁷⁰ conditions ^{26,27}. We thus propose here to apply this approach to incorporate ³H on the surface and/or in the bulk of nanodiamonds for their subsequent labeling.

Detonation NDs provided by Nanocarbon Research Institute (Japan) were exposed to microwave (MW) tritium plasma using ⁷⁵ the experimental MW plasma set-up described elsewhere ²⁵. The

quartz tube was loaded with 17 mg of NDs and then connected to the pumping system and gas inlet. Tritium was then introduced in the tube up to a pressure of 9 mbar, i.e. 6.10^{-6} moles. After a first exposure of 5 min using a 140W injected MW power, oxygen-

⁸⁰ related species desorbed from the NDs during this first plasma treatment were purged by renewing the tritium gas (still 9 mbar). A second plasma exposure of 12 min at 140W was then applied. NDs were cooled down in tritium gas, before being poured into methanol (5 mL). After agitation, the solvent was evaporated.

85 The cleaning operation was repeated twice to allow complete removal of labile tritium. Treated NDs were then stored as dry powder under ambient atmosphere. Considering the two loadings of tritium gas at 9 mbars, an internal volume of the quartz tube of 15.8 mL, and a mean activity of the tritium gas of 58 000 Ci/mol, advections around that the 17 means of NDs means for the store of the

⁹⁰ calculations reveal that the 17 mg of NDs were finally exposed to a total activity of 696 mCi.
 Quantification of ³H incorporation was performed by measuring the radioactivity in the combustion gas of air-annealed ³H-plasma exposed NDs, using liquid scintillation. To identify the diverse
 ⁹⁵ tritium binding states, radioactivity countings were done at different desorption isotherms with long stabilization times (20 h). The radioactivity release from 5mg ³H-NDs according to the temperature threshold and its associated kinetic are shown on

Figure 1. At room temperature, no significant tritium desorption in ambient atmosphere was observed. After 4h at 160°C, only 500 μ Ci/mg were measured in the combustion gas, which rise to 940 μ Ci/mg after 20h at the same temperature. This concentration

- ⁵ represents around 10% of the total radioactivity carried by the treated NDs. At these temperatures, desorption only affect the weakly bonded molecules to the NDs surface (electrostatic adsorption, hydrogen bonds, etc...). Nevertheless, this observation is of outmost importance as it confirms the stability
- ¹⁰ of the association of ³H with NDs for further biological assays. After a following step at 400°C for an additional 20h, 7630 μ Ci/mg were released, i.e. corresponding to 83% of the total radioactivity. At this temperature threshold, a strong oxidation occurs with the formation of carbonyls and carboxylic groups ²⁸
- ¹⁵ and covalent surface terminations are desorbed. This observation confirms that the major part of tritium labelling can be associated with ³H strongly bonded at the surface of the NDs. However, part of the radioactivity still remains in the diamond core that can be released after a final annealing at 600°C, a temperature at
- ²⁰ which NDs are entirely burned away. Accordingly, the total radioactive activity of ³H-NDs is estimated to 9120±120 µCi/mg. From these data, we inferred that this stable radioactive labeling of ND not only results from surface C-³H bonds but also from the diffusion of ³H deep inside the diamond lattice. The total
- ²⁵ subsequent activity released during the 160°C and 400°C annealings enable to estimate that 93% of the tritium atoms were bound to the ND surface, thus 7% are buried in the diamond core. This indicates that the tritium diffusion within the diamond matrix is active during this treatment as was previously reported
- $_{30}$ for hydrogen in bulk diamond 26,27 . Furthermore, this embedded $^3\mathrm{H}$ represents a major advantage in the particular case of surface functionalization of $^3\mathrm{H}\text{-NDs}$, that would have led to the total or partial replacement of C- $^3\mathrm{H}$ surface terminations. Part of the tritium being implanted within the nanodiamond lattice, β^-
- ³⁵ activity measurement will thus be directly related to ND concentration, allowing accurate ND quantification in tissues. Indeed, pharmacokinetic studies can be carried out with a total activity of only 1 μCi per mice, as reported in Couvreur et al. paper ²¹. Thus, with more than 600 μCi/mg remaining in the
- ⁴⁰ particle core even after complete surface oxidation, our ³H-NDs will perfectly match the biodistribution requirements in terms of activities and concentration. Furthermore, beyond the synthesis of radioactive labeled NDs for biological application, these experiments also reveal the very high loading capacity of NDs
- ⁴⁵ with tritium, and consequently with hydrogen. Starting from 696 mCi injected in the quartz tube, desorption treatments demonstrates that the 17 mg of treated NDs finally exhibit a total activity of 155 mCi, i.e. an incorporation yield of 22%. Obviously, this high adsorption capacity is directly linked with
- ⁵⁰ the specific surface area of our nanomaterial. Considering a value of 350 m²/g we measured ⁷ and 17 mg of NDs, a mean density of 5.10^{13} ³H/cm² is obtained for tritium concentration at NDs surface. As a comparison, note that the hydrogen concentration obtained on a 2x1 reconstructed (100) diamond surface saturated
- ss with hydrogen ²⁹ is 1.10¹⁵ H/cm². This means that, despite harsh plasma conditions to modify their surface, only 1 carbon atom over 20 seems to be linked to tritium on our NDs. Here, the effectiveness of such plasma treatments on NDs and certainly on NDs aggregates requires further investigation. However, this
- ⁶⁰ result appears as essential to better understand the surface reactivity of NDs, while hydrogenation of nanodiamonds focuses an intense research effort notably toward photocatalysis application as recently reported in Hamers ³⁰ and Nebel ³¹ papers.



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Figure 1. Radioactive titration of tritium released from ³H-NDs (blue ⁷⁵ circles: Experimental. points) after three sequential annealing treatments in air at increasing temperatures. The dotted red line indicates the temperature measured in the crucible.

The surface chemistry of ³H-NDs was characterized using FTIR spectroscopy. Using a similar approach as previously reported for ⁸⁰ conventional hydrogenated NDs preparation, here ³H-NDs were incorporated in a KBr pellet (2%wt) for transmission analysis. FTIR spectra of as-received NDs and ³H-NDs are reported in Figure 2. Both samples exhibit strong features at 3400 and 1630 cm⁻¹ which originate from adsorbed water in the KBr pellet and ⁸⁵ on NDs ²⁸ and a contamination with CO₂ around 2375 cm⁻¹. Note that due to the radioactivity of the sample, the in-situ annealing of the KBr pellet we usually performed to remove this adsorbed water was not applied here. An additional feature is also visible around 2160 which is not attributed yet. As-received NDs exhibit ⁹⁰ a characteristic C=O stretching band at 1720 cm⁻¹, linked to carbonyl and/or carboxylic groups ³². C-H stretching are also clearly visible around 2900 cm⁻¹, typical signature of amorphous carbon adsorbed on the nanodiamond. After treatment, the disappearance of the C=O stretching band at 1720 cm⁻¹ confirms 95 the desorption of the oxidized terminations during the ³H-plasma exposure. This is in agreement with our previous plasma hydrogenation studies ^{24,33}. Surprisingly, C-H features do not disappear after ³H-plasma treatment. In fact, a part of this C-H stretching band could result from organic contamination of the ¹⁰⁰ sample ³⁴, although it can also be assumed that some C-H terminations remain on NDs even after such H-plasma treatment. Concerning the formation of such C-³H stretching bands, FTIR experiments with ³H are poorly described in the literature. Based on Sun and Sidhu works^{35,36}, we calculated the C-³H stretching ¹⁰⁵ frequencies with respect to C-¹H bands using harmonic potential approximation and reduced mass ratios (equation 1): in our case, a ratio of 0.62 is obtained, which leads to a C-³H stretching most likely to be localized around 1800 cm⁻¹. On the observed FTIR spectrum, no clear features are visible around such wavenumbers ¹¹⁰ after ³H treatment, which is not at first glance in agreement with the creation of C-³H terminations. However, as explained by Sidhu et al. 36, a very weak signal intensity of the C-3H stretching bands is expected, since the integrated intensity is inversely proportional to the reduced mass of the oscillator. Moreover, 115 tritium coverage represents 5% of the carbon atoms. Here, a clear spectroscopic evidence of the formation of C-³H terminations after our ³H-plasma treatment is thus not allowed. Nevertheless, the desorption of the carboxylic functions revealed by FTIR, which proves the reactivity of the ³H plasma together with the 120 stable radioactivity observed up to 400°C of our treated NDs definitely support the formation of such C-³H terminations.

$$\frac{\omega_{C_T}}{\omega_{C_T}} = \sqrt{\frac{m_H(m_T + M_C)}{m_T(m_H + M_C)}}$$

equation (1)



Figure 2 FTIR spectrum of ³H-NDs compared to as received NDs

- In conclusion, we reported here for the first time a very ⁵ straightforward, efficient and scalable approach enabling radiolabeling of NDs using tritium MW plasma. The results demonstrate the excellent stability of tritium incorporated into NDs which can be even diffusing through the inner core of the particles. A major advantage of this approach rely in the ¹⁰ possibility to keep a high activity concentration in the ND core,
- suitable for biodistribution studies, which will remains unaffected even after subsequent functionalization of the ND surface. While such β - activity will be directly related to 3H-NDs concentration, this powerful approach to produce radiolabeled NDs in large 15 quantity (up to hundreds of mg) does now appear as a very
- efficient tool to evaluate the biodistribution and the pharmacokinetics studies of nanodiamonds in tissues.

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